

Improved Fuzzy C-Means for Brain Tissue Segmentation Using T1-Weighted MRI Head Scans

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Image segmentation is the process of partitioning a digital image into non-overlapped, consistent regions that are homogeneous attributes with respect to some characteristics like gray level, color, tone or texture, motion etc. Image segmentation is an important and challenging

Abstract :-

Brain tissue segmentation of Magnetic Resonance Imaging (MRI) is an important and one of the challenging tasks in medical image processing. MRI images of brain are classified into two types: classifying tissues, anatomical structures. It comprised into different tissue classes which contain four major regions, namely Gray matter (GM), White matter (WM), Cerebrospinal fluid (CSF), and Background (BG). The present study of proposed method is an improved fuzzy c-means (FCM) clustering for tissue segmentation using T1-weighted head scans. The proposed method improved by modifying the objective function, cluster center and membership value for updating criterion. The quantitative measures of results were compared using the metrics Dice Coefficient (DC) and processing time. The DC value of proposed method attained maximum value while compared to conventional FCM. The proposed method is very efficient and faster than FCM for brain tissue segmentation from T1-weighted head scans.

Keywords: Brain MRI, Clustering, Fuzzy c-means, Image Segmentation.

1. Introduction

problem and used in various applications like object recognition, traffic control systems, geographical imaging and medical imaging [1] [2]. Several image segmentation approaches have been proposed and it is classified into edge detection, thresholding, clustering and region based methods. The proposed work is focused on the region based approach using fuzzy c-means (FCM) clustering. FCM clustering algorithm is a soft segmentation method that retains more information from the input images. It is proved to be the best method for the anisotropic nature of volumes [3] Segmentation of brain tissues in MRI (Magnetic Resonance Imaging) images plays a significant role in medical image analysis and related operations. Medical imaging provides effective and non-invasive mapping of human soft tissue anatomy. In the field of medicine, good segmentation assists clinicians and patients by providing important information for 3-D visualization, surgical planning and early disease recognition [4]. The diagnostic capability of medical experts improved significantly with the arrival of medical imaging techniques such as computed tomography (CT), positron emission tomography (PET), magnetic resonance (MR) images and single photon emission computed tomography (SPECT). MR images of brain are

classified into two types: classifying tissues, anatomical structures. It comprised into different tissue classes that contain four major regions, namely gray matter (GM), white matter (WM), cerebrospinal fluid (CSF), and background (BG) [5]. In recent years, many approaches have been developed to the brain tissue segmentation and analysis. Benaichouche et al. [6] proposed an improvement method for image segmentation using the FCM clustering algorithm. This algorithm is widely experimented in the field of image segmentation with very successful results. This proposed method, named improved spatial fuzzy c-means (IFCMS) compared to the most used FCM-based algorithms of the literature. Sayed et al. [7] proposed a summarized hybrid techniques for the classification of the MR human brain tissue. The hybrid technique consists of three methods, feature extraction, dimensionality reduction, and classification. FCM used to classify the subjects as normal or abnormal MRI images. Ahmed et al. [8] proposed a summarized hybrid approach for classification of brain tissues in MRI based on genetic algorithm (GA) and support vector machine (SVM). A wavelet based texture feature set derived for classification. The optimal texture features are extracting from normal and tumor regions by using spatial gray level dependence method (SGLDM). The optimal feature set extracted by applying GA. The feature set containing five features and they were inputs to the SVM classifier. This algorithm is advance, to replace the neighborhood term of FCM_S. Thus the execution times of both FCM_S1 and FCM_S2 are considerably reduced.

Shasidhar et al. [10] proposed a FCM algorithm and proved to be superior over the other clustering approaches in terms of segmentation efficiency. In this paper, the application of modified FCM algorithm for MR brain tumor detection is explored. Feature

vector space is used for the segmentation technique. Comparative analysis in terms of segmentation efficiency and convergence rate is performed between the conventional FCM and the modified FCM. The modified FCM algorithm is a fast alternative to the traditional FCM technique.

Yambal and Gupta [11] proposed a survey for the brain tumor detection using segmentation methods. It is based on hierarchical self-organizing map (SOM). The proposed method used FCM technique with histogram based centroid initialization for brain tissue segmentation in MRI of heads scans, FCM algorithm is used in various tasks of pattern recognition, data mining, image processing, gene expression, data recognition etc.,. Modifying and generalizing the FCM algorithm is a prevailing research stream in fuzzy clustering in recent decades. Low depth of field is a method used to give special importance to a part of image which is essential or which has to be focused. In SOM, the first part consists of capturing an image form the database and the second part consists of accurately identify the principle structures in these image volumes.

Hussian [12] proposed a method named improved fuzzy possibilistic c-means (IFPCM). The proposed method combines the FCM and possibilistic c-means (PCM) functions without considering any spatial constraints on the objective function. It is realized by modifying the objective function of PCM algorithm. This proposed algorithm is evaluated and compared with the most popular modified probabilistic c-means techniques via application to simulated MRI brain images corrupted with noise. The quantitative results suggested that the proposed algorithm yields better segmentation results than the others for all tested images.

Vasuda and Satheesh [13] proposed an FCM and MFCM method and that can be successively segmented a tumor provided the parameters are chosen properly. The advance, to replace the neighborhood term of FCM_S. Thus the execution times of both FCM_S1 and FCM_S2 are considerably reduced.

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that minimize dissimilarity (objective) function [18] [19]. The objective function is,

$$J_m = \sum_{j=1}^n \sum_{i=1}^c u_{ij}^m d_{ij}^2(x_j, c_i)$$

where, $m \in [1, \infty]$ is a weighting exponent

$u_{ij} \in [0, 1]$ is the degree of membership function matrix

$d_{ij} = \sqrt{(x_j - c_i)^2}$ - is the Euclidean distance between element

x_j and center of cluster

c_i - is the number of cluster n - is the number of data

The updated membership functions are defined as follows [5], $\mu_{ij} =$

$$\mu_{ij} = \frac{1}{\sum_{l=1}^c \left(\frac{d(x_j, c_l^{(k-1)})}{d(x_j, c_l^{(k)})} \right)^{\frac{2}{m-1}}}$$

$$c_i^{(k)} = \frac{\sum_{j=1}^N (\mu_{ij}^{(k)})^m x_j}{\sum_{j=1}^N (\mu_{ij}^{(k)})^m}$$

This condition will stop if the improvement of the objective function over the previous iteration is below critical value, $\epsilon [1, 0]$. This algorithm is iteratively updating the centers and membership grades for each data point. FCM iteratively moves the cluster centers to the right location within a data set. The detailed FCM algorithm is given below.

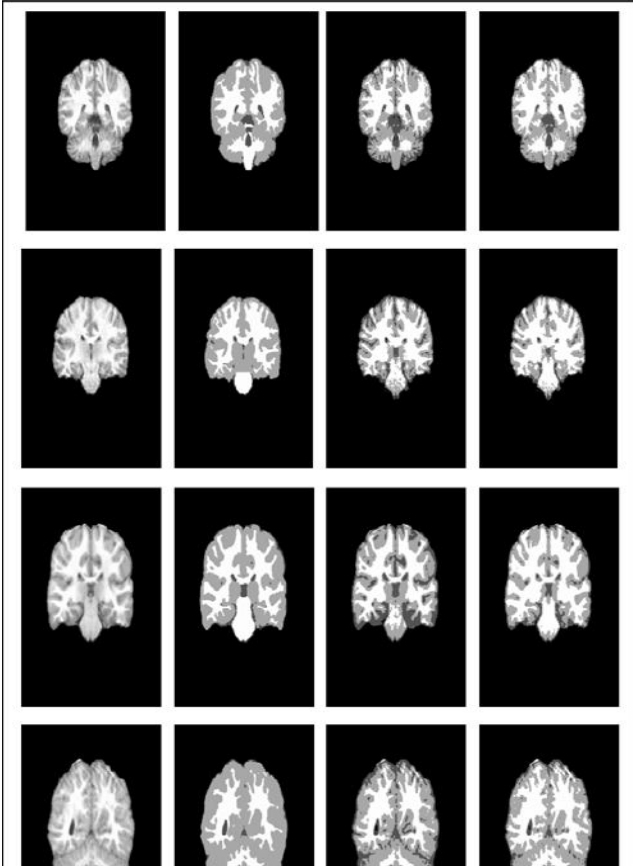
Requirement: Set values for the number of clusters C , the degree of fuzziness $m > 1$ and the error \sum .

Step 1: Initialize randomly the centers of clusters $c_i(0)$.

Step 2: $k \leftarrow 1$

Step 3: repeat

Step 4: Calculate the membership matrix $U(K)$ using



database [20]. Both qualitative and quantitative validations were used for the performance evaluation. Experiments were done by taking the MRI brain image applied to the qualitative validation in the form of visual inspection with some of the sample T1-weighted images MRI and results are shown in Figure 1. The original images are shown in column 1, the corresponding ground truth images are in column 2, the results of FCM in column 3 and the results of proposed method are in column 4. The proposed method gives better results than the conventional FCM method.

Figure 1. Original images are in column 1, corresponding ground truth images are in column 2, results of FCM are in column 3 and results of proposed method are in column 4. For the quantitative validation, the performance is checked against two parameters. They are Dice Coefficient (DC) and processing time. The parameter DC is used to verify the similarity between the ground truth and

the result of proposed work. The value for DC ranges from 0 to 1 where 0 for no agreement and 1 for exact agreement.

The DC is given by:

$$D(A, B) = \frac{2|A \cap B|}{|A| + |B|} \quad (13)$$

where, A represents the ground truth image and B represents the proposed result image.

Table 1 shown the DC value of conventional FCM and proposed method calculates with 18 IBSR volumes. The proposed method gives the average values for GM is 0.84, WM is 0.86 and CSF is 0.13. The proposed method gives better results while compared to the conventional FCM clustering. The graphs given in Figure 2 shows the quantitative representation of DC value for FCM and IFCM with bar representation. In Figure 3, the X axis represents MRI volume number considered for experiment and Y axis represents the processing time of FCM and IFCM.

Table 1. DC values of GM, WM and CSF for conventional FCM and Improved FCM.

Volume Id	FCM			Improved FCM		
	CSF	GM	WM	CSF	GM	WM
IB_1	0.17	0.77	0.78	0.22	0.74	0.80
IB_2	0.26	0.77	0.80	0.29	0.79	0.83
IB_3	0.08	0.76	0.83	0.12	0.85	0.89
IB_4	0.07	0.73	0.85	0.08	0.84	0.89
IB_5	0.08	0.71	0.79	0.09	0.81	0.85
IB_6	0.10	0.66	0.84	0.14	0.83	0.92
IB_7	0.06	0.85	0.88	0.14	0.87	0.90
IB_8	0.06	0.83	0.89	0.14	0.84	0.88
IB_9	0.13	0.82	0.84	0.17	0.87	0.87
IB_10	0.08	0.85	0.94	0.14	0.87	0.95

IB_11	0.08	0.85	0.88	0.14	0.86	0.90
IB_12	0.15	0.87	0.83	0.18	0.84	0.85
IB_13	0.08	0.77	0.83	0.03	0.85	0.88
IB_14	0.04	0.78	0.84	0.03	0.85	0.86
IB_15	0.02	0.78	0.85	0.10	0.84	0.86
IB_16	0.10	0.73	0.73	0.11	0.80	0.71
IB_17	0.05	0.76	0.81	0.08	0.84	0.84
IB_18	0.09	0.74	0.75	0.14	0.82	0.79
Average	0.09	0.78	0.83	0.13	0.83	0.86

Then average processing time of each method is converted into percentage (%) using the below equation.

$$Time\ difference\ (\%) = \frac{HT - LT}{HT} * 100 \quad (14)$$

where HT is representing the higher time and LT

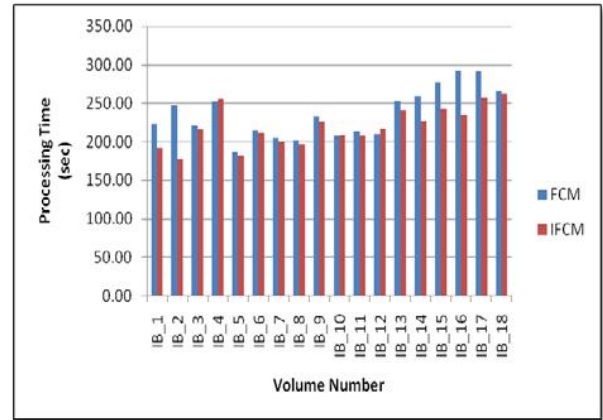
is represent

Table 2. Processing time for conventional FCM and Improved FCM.

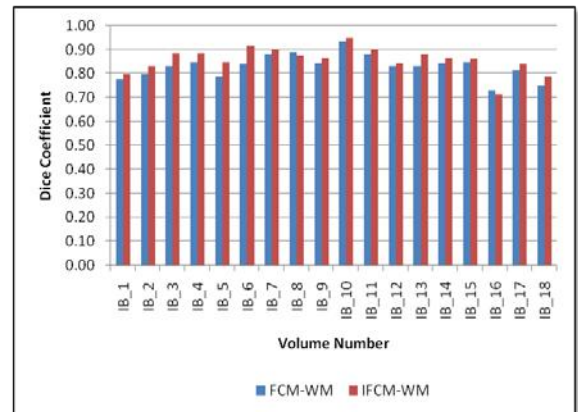
Volume Id	FCM (sec)	Improved FCM (sec)
IB_1	223.48	192.02
IB_2	247.63	177.46
IB_3	221.38	215.73
IB_4	252.63	255.87
IB_5	186.14	181.84
IB_6	215.08	211.62
IB_7	206.03	199.06
IB_8	201.44	196.95
IB_9	233.22	225.26
IB_10	207.36	209.18
IB_11	213.36	207.97
IB_12	209.84	217.49
IB_13	252.79	241.40
IB_14	259.28	226.92

IB_15	277.34	242.80
IB_16	292.24	235.88
IB_17	291.51	256.69
IB_18	266.15	263.26
Average	236.49	219.86

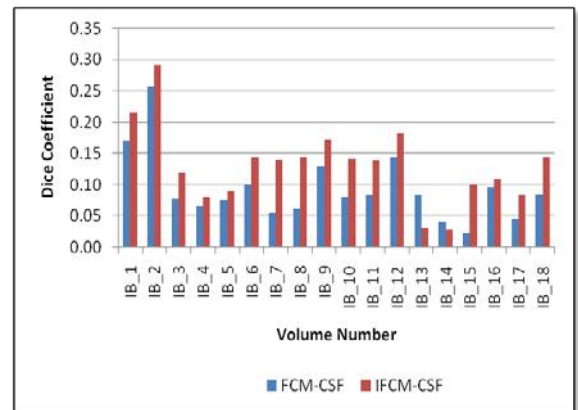
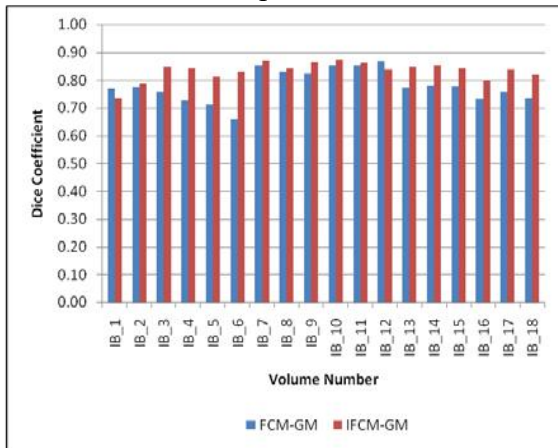
Table 2 is shown the processing time taken by conventional FCM and improved FCM for the 18 IBSR volumes. The proposed method takes minimum time while compared to conventional FCM clustering. In Figure 4, X axis represents the volume numeral Y axis represents the processing time in seconds. After applying the average processing time values in above equation (14), the proposed method is 7% faster than the conventional FCM. Our proposed method is fast as well as given satisfied results for T1-weighted images while compared with existing conventional technique.



(a)



(b)



(c)

Figure 2. DC Measurement Graph (a) GM values for FCM and IFCM (b) WM values for FCM and IFCM and (c) CSF values for FCM and IFCM

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